

Improving spacer delivery for low flow (paediatric) use.

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Background

- Children struggle to coordinate pMDI actuation with correct inhalation.
- Receipt of drug via tidal breathing is an attractive solution.
- All paediatric pMDI users should have a spacer or valved holding chamber (VHC).
- What factors are important when choosing a VHC — recommendation, prescription status, practicality, lung function ?

Introduction

- Selection is rightly influenced by scientific evaluation. However :
 - ♦ usual 30L/min flow rate assessments do not represent paediatric tidal breathing.¹
 - ♦ at low flow rates, VHCs with open exhaust valves 'steal' inspired air and reduce drug lung deposition (**Figure 1**).²

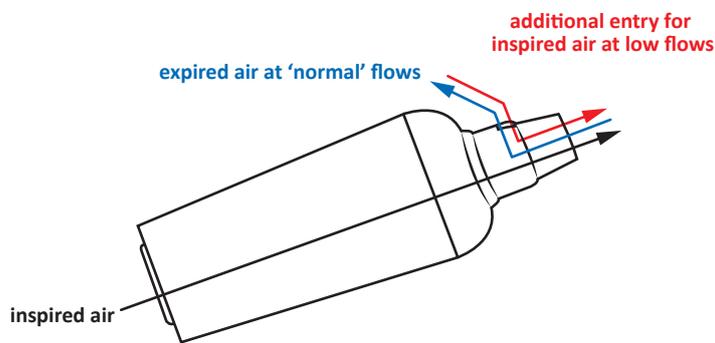


Figure 1 - VHC routes of air flow

Objectives

- Valve technology research to improve Able Spacer®-2 function at low flow rates.
- Deliver improved utility for young children.

Assessments

- Exemplar pMDI - 100µg salbutamol (Ventolin Evohaler®).
- Standard flow 30L/min Next Generation Impactor aerosol performance.
- Low flow 10L/min Dosage Unit Sampling Apparatus (DUSA) quantifying drug retention within the VHC.
- Three Able Spacer-2 valve assembly comparisons plus Ventolin pMDI alone.

References

1. Mitchell JP, Nagel MW. In vitro performance testing of three small volume-holding chambers under conditions that correspond with use by infants and small children. J Aerosol Med 1997; 10 (4): 341-349 (<https://doi.org/10.1089/jam.1997.10.341>, accessed 14/09/2017).
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3. Oliveira RF, Silva MV, Teixeira SFCF, Cabral-Marques HM, Teixeira JCF. Efficiency of valved holding chambers: experimental full dose assessment. J Aerosol Med Pulmon Drug Del 2015; 28: A-2. Full poster available on researchgate.net

Development work

Able Spacer-2 VHC mouthpiece and valve

| Current | | Development examples |
|---------|--|----------------------|
| | Valve — additional cuts and shape change | |
| | Valve and chamber top support — exit port enlarged (circled) | |
| | New two-piece valve support — closes during inhalation | |

Results

| | Fine Particle Fraction (<5µm) | Fine Particle Dose (µg<5µm) |
|-----------------|-------------------------------|-----------------------------|
| pMDI only | 47.9 ± 2.4 | 41.7 ± 4.4 |
| + Current valve | 55.0 ± 2.0 | 55.8 ± 9.2 |
| + Development-1 | 51.8 ± 2.4 | 52.2 ± 9.9 |
| + Development-2 | 55.4 ± 2.5 | 53.1 ± 10.3 |

Table 1 - Similar key aerosol characteristics at 30 L/min (mean ± SD)

| | µg recovered per actuation | % recovered of emitted dose |
|-----------------|----------------------------|-----------------------------|
| pMDI only | 82.1 ± 5.8 | ≅ 100.0 |
| + Current valve | 43.6 ± 6.5 | 49.4 ± 6.3 |
| + Development-1 | 45.1 ± 2.8 | 56.6 ± 4.4 |
| + Development-2 | 52.7 ± 4.5 | 58.0 ± 2.1 |

Table 2 - Improved DUSA recovery at 10 L/min (mean ± SD)

Conclusions

- "In vitro measurements made at constant high flow rates in excess of 20 L/min do not reveal [these] differences in performance that are clinically significant, and may lead the physician to prescribe a device that under certain conditions may not deliver any drug to infants or small children."¹
- At low flow rates, the current research demonstrates improved performance using new valve assemblies.
- The data also demonstrate improvements on previous low flow, dose uniformity comparator research.³

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